



## Editorial

## Do we really need another individual coronary plaque characterization measurement?



## Keywords:

Atherosclerosis  
Imaging

Non-calcified coronary artery plaques with a large necrotic core covered by a thin fibrous cap are among the most vulnerable to rupture and precipitate an acute coronary syndrome (ACS) (Fig. 1A) [1,2]. These higher-risk “lipid-rich” plaques have lower attenuation values [measured in Hounsfield units (HU)] by coronary CT angiography (CCTA) than lower-risk “fibrous” plaques. However, HU values within individual plaques vary, resulting in significant overlap between lipid-rich and fibrous plaques [3]. Moreover, HU values are influenced by inherent, test-specific characteristics including adjacent intraluminal contrast concentration and image reconstruction techniques [4,5].

Given the difficulty in establishing a simple HU cut-off value for differentiating lipid-rich from fibrous plaques, Nakajima and colleagues, in this issue of *Atherosclerosis*, explored the clinical feasibility of using effective atomic number (EAN) values [6]. This novel tissue density-independent measurement was derived from single-source dual-energy CT, which recently has been shown to significantly reduce beam-hardening artifacts and improve image quality of CCTA [7,8]. In their study, Nakajima et al. included 11 patients who underwent single-source dual-energy CCTA and intravascular ultrasound (IVUS) imaging. Using established IVUS criteria, the authors classified 44 non-calcified coronary artery plaques as either fibrous ( $n = 13$  plaques) or soft ( $n = 29$  plaques) (Fig. 1B). The mean HU value and the mean EAN value for soft plaques were both significantly lower in soft plaques *versus* fibrous plaques. However, on receiver operating characteristic analysis for classifying soft *versus* fibrous plaque as defined by IVUS, the area under the curve for mean effective atomic number value was significantly greater (0.91; 95% confidence interval 0.73–0.97) than for mean HU value (0.79; 95% confidence interval 0.60–0.90;  $p = 0.046$ ).

These findings from Nakajima et al. are novel in their suggestion that EAN values derived from single-source dual-energy CCTA may

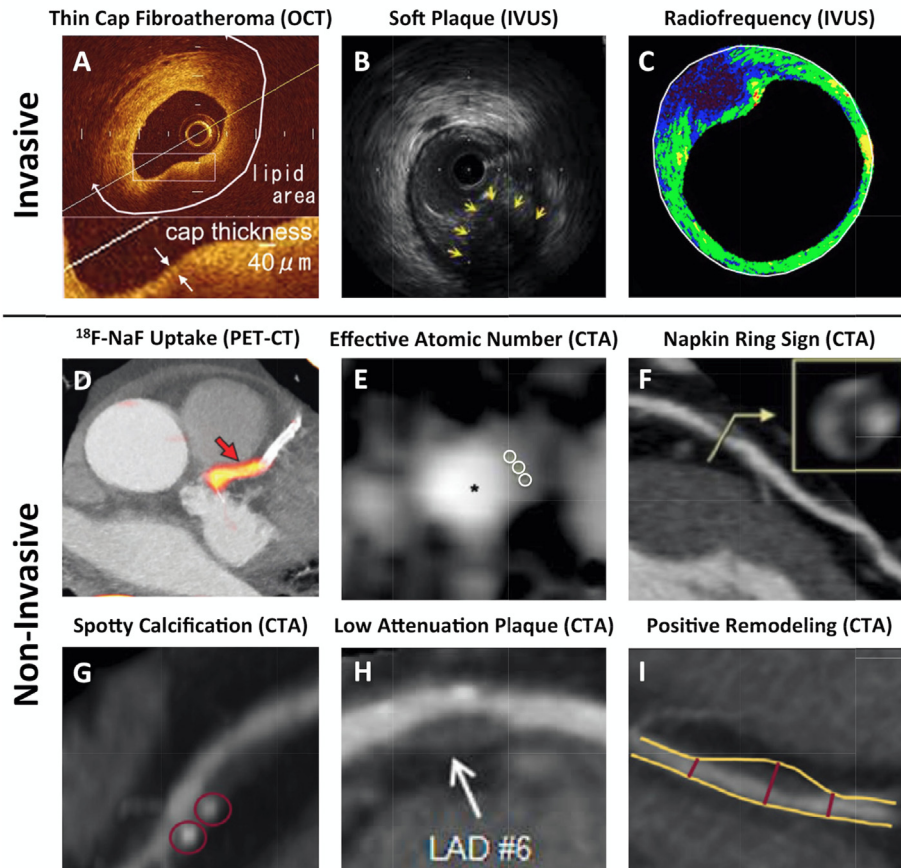
be a clinically useful alternative to HU values for differentiating soft and fibrous non-calcified plaques on CCTA. The fact that the authors were able to find a statistically significant difference in the receiver operating characteristic analysis for classification with such a small cohort suggests a strong signal. Furthermore, their data are remarkably similar to previously published findings that single-source dual-energy-derived EAN can help differentiate between soft and fibrous non-calcified carotid artery plaques [9]. Overall, the strength of these novel data warrant additional investigation in a larger patient population.

Given that single-source dual-energy CCTA is still limited in clinical use, it may be quite some time before such a follow-up study could be performed. Furthermore, EAN should be compared against newer automated plaque quantification software tools that have been shown to improve HU value measurement compared with manual analysis [10]. Comparing against a more accurate measurement of CT-derived HU values may attenuate the apparent advantage of EAN in differentiating soft and fibrous plaques. Moreover, comparison to data using intravascular ultrasound radiofrequency (IVUS-RF) analysis (Fig. 1C) [11,12] or newer approaches with  $^{18}\text{F}$ -sodium fluoride uptake on positron emission tomography (PET) may also help identify high-risk coronary plaques (Fig. 1D) [13]. Future studies could also compare EAN (Fig. 1E) to a broad range of CCTA-identified ‘high-risk’ plaque features that have been associated with future ACS (i.e. ‘napkin-ring’ sign, spotty calcification, positive remodeling, and low attenuation plaque; Fig. 1F–I). Unfortunately, such features have limited positive predictive value for future ACS when compared to CCTA-derived luminal stenosis [14] or coronary plaque volume alone [15–17]. In this context, it is unclear whether EAN will significantly improve our ability to predict ACS beyond available plaque measures. To prove the independent and incremental value of EAN, future studies should focus on the requirements of a good prognostic test. Namely, outcomes-based validation and reliability studies are needed to prove new techniques can identify patients at low-risk for adverse events, define clear gradations of risk, and concentrate risk in patients with an abnormal test [18].

In summary, the findings of Nakajima et al. are novel and provocative. Their suggestion, that single-source dual-energy-derived effective atomic number values may better differentiate between soft and fibrous non-calcified plaques on CCTA than HU values, needs to be further validated in a larger cohort, in a study that ideally uses automated plaque quantification software for HU value measurement, includes comparison against the broad range of individual plaque measures already available, and establishes independent and incremental predictive value for relevant patient outcomes.

DOI of original article: <http://dx.doi.org/10.1016/j.atherosclerosis.2017.03.025>.

<http://dx.doi.org/10.1016/j.atherosclerosis.2017.04.012>  
0021-9150/© 2017 Elsevier B.V. All rights reserved.



**Fig. 1.** Examples of plaque measures identified by invasive and non-invasive imaging.

(A) Optical coherence tomography (OCT) showing a thin-cap fibroatheroma (reproduced with permission [2]), (B) intravascular ultrasound (IVUS) identified soft plaque (yellow arrows; reproduced with permission [6]), (C) color-coded integrated backscatter IVUS images of a coronary artery plaque and overlying fibrous cap [fibrous (green), dense fibrosis (yellow), lipid pool (blue and purple), calcification (red); reproduced with permission [19]], (D) positron emission tomography computed tomogram (PET-CT)-identified  $^{18}\text{F}$ -sodium fluoride (NaF) uptake at the site of a culprit plaque (red arrow; reproduced with permission [13]), (E) coronary computed tomography angiography (CCTA)-identified effective atomic number (EAN) (reproduced with permission [6]), (F) CCTA-identified 'napkin ring sign' (reproduced with permission [20]), (G) CCTA-identified spotty calcification (reproduced with permission [14]), (H) CCTA-identified low attenuation plaque (reproduced with permission [16]), (I) CCTA-identified positive remodeling (reproduced with permission [14]) (For interpretation of the references to colour in this figure legend, the reader is referred to the web version of this article.)

## Conflict of interest

The authors declared they do not have anything to disclose regarding conflict of interest with respect to this manuscript.

## References

- [1] J. Narula, P. Garg, S. Achenbach, S. Motoyama, R. Virmani, H.W. Strauss, Arithmetic of vulnerable plaques for noninvasive imaging, *Nat. Clin. Pract. Cardiovasc Med.* 5 (Suppl 2) (2008) S2–S10.
- [2] T. Ito, M. Terashima, H. Kaneda, et al., Comparison of in vivo assessment of vulnerable plaque by 64-slice multislice computed tomography versus optical coherence tomography, *Am. J. Cardiol.* 107 (9) (2011) 1270–1277.
- [3] K. Pohle, S. Achenbach, B. Macneill, et al., Characterization of non-calcified coronary atherosclerotic plaque by multi-detector row CT: comparison to IVUS, *Atherosclerosis* 190 (1) (2007) 174–180.
- [4] S. Achenbach, K. Boehmer, T. Pflederer, et al., Influence of slice thickness and reconstruction kernel on the computed tomographic attenuation of coronary atherosclerotic plaque, *J. Cardiovasc Comput. Tomogr.* 4 (2) (2010) 110–115.
- [5] S. Suzuki, S. Furui, S. Kuwahara, et al., Accuracy of attenuation measurement of vascular wall in vitro on computed tomography angiography: effect of wall thickness, density of contrast medium, and measurement point, *Invest. Radiol.* 41 (6) (2006) 510–515.
- [6] S. Nakajima, H. Ito, T. Mitsuhashi, Y. Kubo, K. Matsui, I. Tanaka, R. Fukui, H. Omori, T. Nakaoka, H. Sakura, E. Ueno, H. Machida, Clinical application of effective atomic number for classifying non-calcified coronary plaques by dual-energy computed tomography, *Atherosclerosis* 261 (2017) 138–143.
- [7] T.A. Fuchs, J. Stehli, M. Fiechter, et al., First experience with monochromatic coronary computed tomography angiography from a 64-slice CT scanner with Gemstone Spectral Imaging (GSI), *J. Cardiovasc Comput. Tomogr.* 7 (1) (2013) 25–31.
- [8] J.A. Scheske, J.M. O'Brien, J.P. Earls, et al., Coronary artery imaging with single-source rapid kilovolt peak-switching dual-energy CT, *Radiology* 268 (3) (2013) 702–709.
- [9] Y. Shinohara, M. Sakamoto, K. Kuya, et al., Assessment of carotid plaque composition using fast-kV switching dual-energy CT with gemstone detector: comparison with extracorporeal and virtual histology-intravascular ultrasound, *Neuroradiology* 57 (9) (2015) 889–895.
- [10] D. Dey, T. Schepis, M. Marwan, P.J. Slomka, D.S. Berman, S. Achenbach, Automated three-dimensional quantification of noncalcified coronary plaque from coronary CT angiography: comparison with intravascular US, *Radiology* 257 (2) (2010) 516–522.
- [11] K. Sano, M. Kawasaki, Y. Ishihara, et al., Assessment of vulnerable plaques causing acute coronary syndrome using integrated backscatter intravascular ultrasound, *J. Am. Coll. Cardiol.* 47 (4) (2006) 734–741.
- [12] S.K. Mehta, J.R. McCrary, A.D. Frutkin, W.J. Dolla, S.P. Marso, Intravascular ultrasound radiofrequency analysis of coronary atherosclerosis: an emerging technology for the assessment of vulnerable plaque, *Eur. Heart J.* 28 (11) (2007) 1283–1288.
- [13] N.V. Joshi, A.T. Vesey, M.C. Williams, et al.,  $^{18}\text{F}$ -fluoride positron emission tomography for identification of ruptured and high-risk coronary atherosclerotic plaques: a prospective clinical trial, *Lancet* 383 (9918) (2014) 705–713.
- [14] S.B. Puchner, T. Liu, T. Mayrhofer, et al., High-risk plaque detected on coronary CT angiography predicts acute coronary syndromes independent of significant stenosis in acute chest pain: results from the ROMICAT-II trial, *J. Am. Coll.*

- Cardiol. 64 (7) (2014) 684–692.
- [15] D.M. Thomas, S. Divakaran, T.C. Villines, et al., Management of coronary artery calcium and coronary CTA, *Find. Curr. Cardiovasc Imaging Rep.* 8 (6) (2015) 18.
- [16] S. Motoyama, M. Sarai, H. Harigaya, et al., Computed tomographic angiography characteristics of atherosclerotic plaques subsequently resulting in acute coronary syndrome, *J. Am. Coll. Cardiol.* 54 (1) (2009) 49–57.
- [17] M.O. Versteyleen, B.L. Kietselaer, P.C. Dagnelie, et al., Additive value of semiautomated quantification of coronary artery disease using cardiac computed tomographic angiography to predict future acute coronary syndrome, *J. Am. Coll. Cardiol.* 61 (22) (2013) 2296–2305.
- [18] R. Hachamovitch, M.F. Di Carli, Methods and limitations of assessing new noninvasive tests: Part II: outcomes-based validation and reliability assessment of noninvasive testing, *Circulation* 117 (21) (2008) 2793–2801.
- [19] M. Kawasaki, An integrated backscatter ultrasound technique for the detection of coronary and carotid atherosclerotic lesions, *Sens. (Basel)*. 15 (1) (2015) 979–994.
- [20] K. Otsuka, S. Fukuda, A. Tanaka, et al., Napkin-ring sign on coronary CT angiography for the prediction of acute coronary syndrome, *JACC. Cardiovasc. imaging*. 6 (4) (2013) 448–457.

Nishant R. Shah

*Division of Cardiology, Department of Medicine, Brown University  
Warren Alpert Medical School, Providence, RI, USA*

Michael K. Cheezum  
*Department of Medicine (Cardiology Service), Fort Belvoir Community  
Hospital, Fort Belvoir, Virginia, USA*

Sadako Motoyama  
*Department of Cardiology, Fujita Health University, Aichi, Japan*

Yiannis S. Chatzizisis\*  
*Cardiovascular Division, University of Nebraska Medical Center,  
Omaha, NE, USA*

\* Corresponding author. Cardiovascular Division, University of  
Nebraska Medical Center, 982265 Nebraska Medical Center,  
Omaha, NE 68198, USA.

*E-mail address:* [ychatzizisis@icloud.com](mailto:ychatzizisis@icloud.com) (Y.S. Chatzizisis).

9 April 2017  
Available online 15 April 2017